

# *Focusing on the Clinical Importance of Conformability*

***Ron Waksman, MD,FACC***

***Professor of Medicine (Cardiology) Georgetown University,***

***Associate Director Division of Cardiology***

***Washington Hospital Center Washington DC***

# Disclosure Statement of Financial Interest

**Within the past 12 months, I or my spouse/partner have had a financial interest/arrangement or affiliation with the organization(s) listed below.**

## **Affiliation/Financial Relationship**

- Grant/Research Support
- Consulting Fees/Honoraria

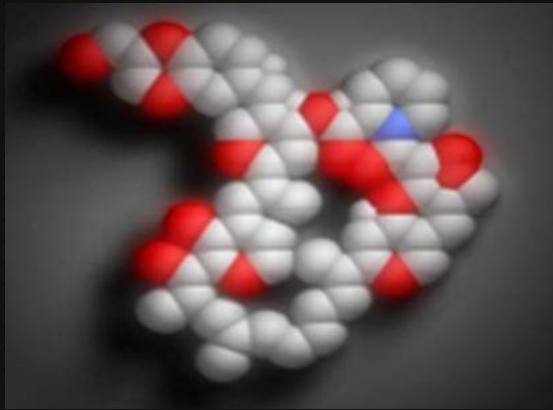
## **Company**

- Volcano
- Medtronic Vascular
- Abbott Vascular
- Boston Scientific
- Biotronik
- Medtronic
- Abbott Vascular
- Boston Scientific
- Lilly Daiichi
- Astra Zeneca

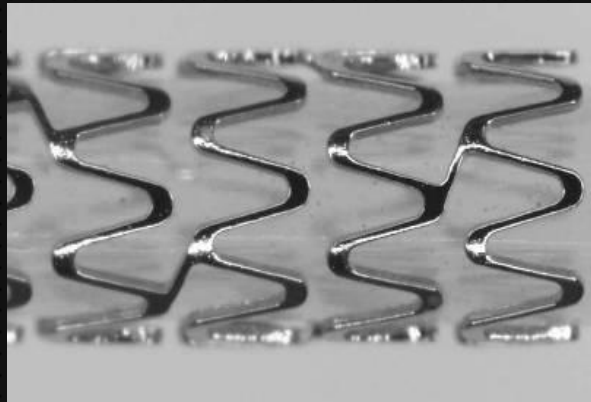
# DES design affects procedural success and clinical outcomes

## Elements of DES Design

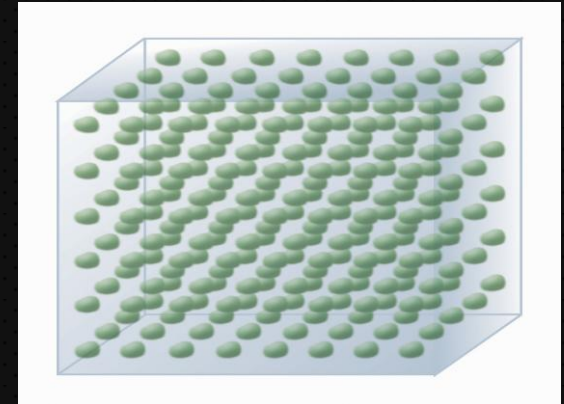
**Drug**



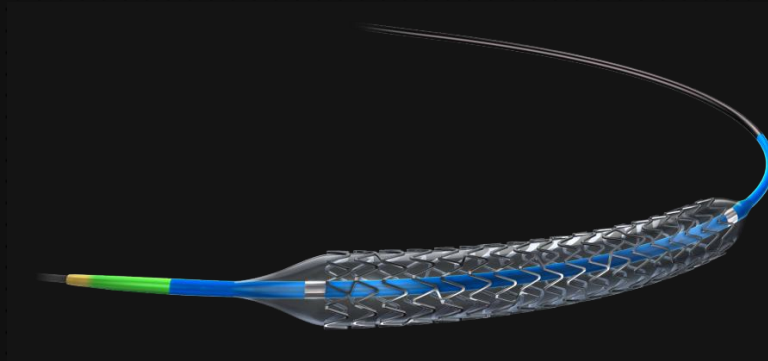
**Scaffold**



**Polymer**



**Delivery System**



# The Value of Thin Stent Struts

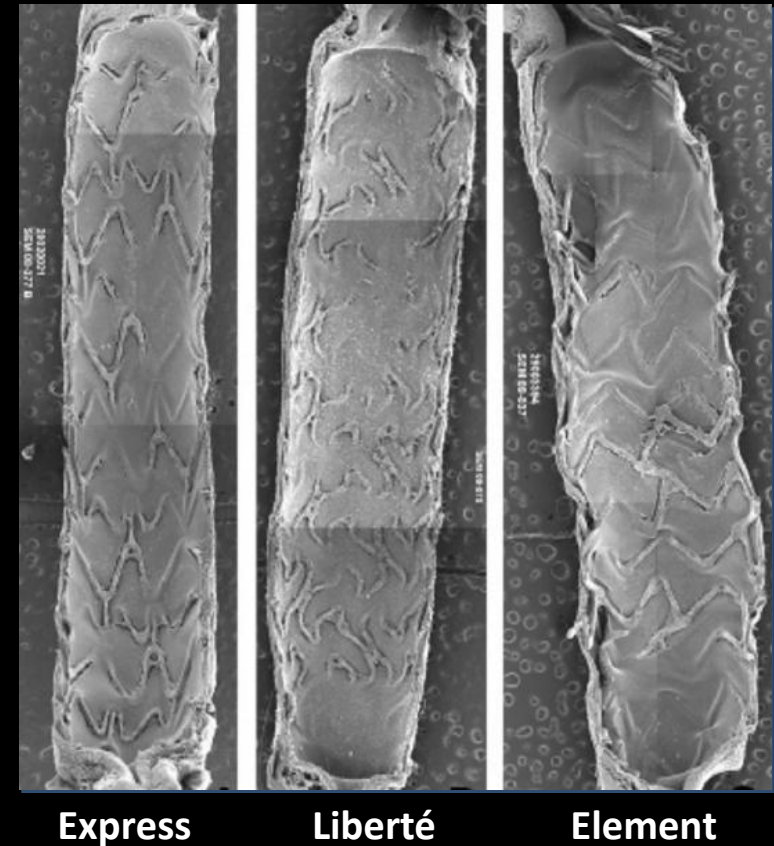
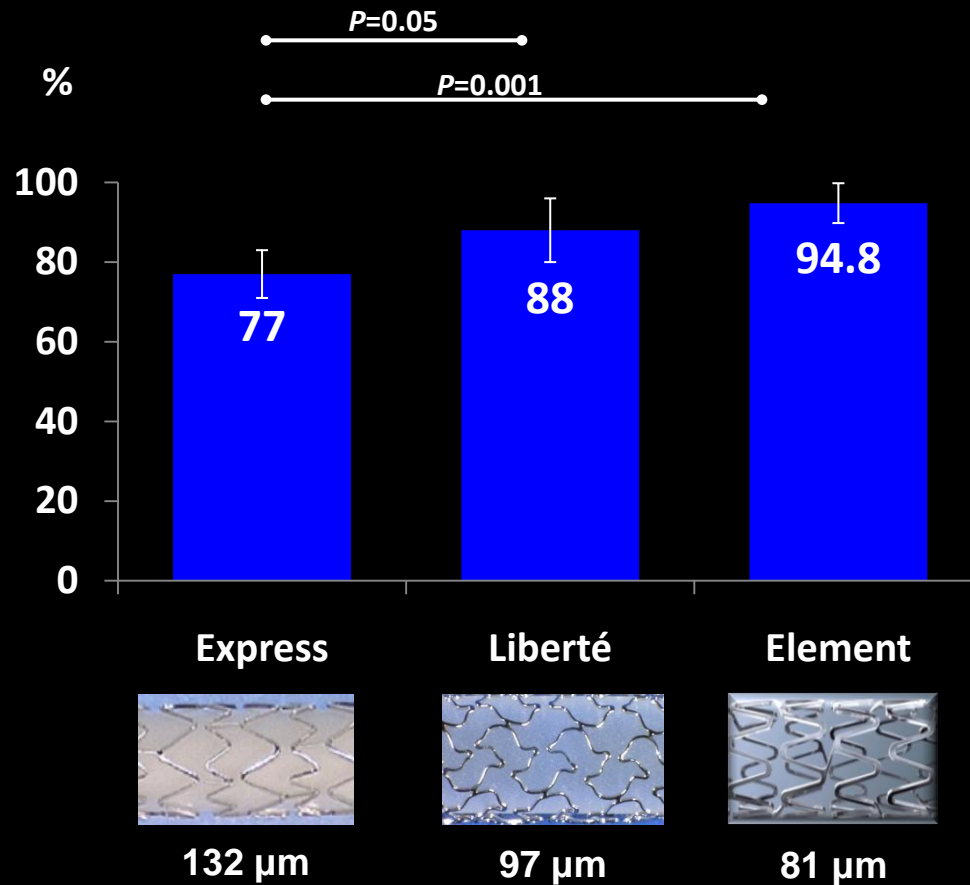
- PreClinical Models have demonstrated



- Reduced acute injury
- Reduced inflammation
- Rapid incorporation of struts within neointima
- Rapid re-endothelialization

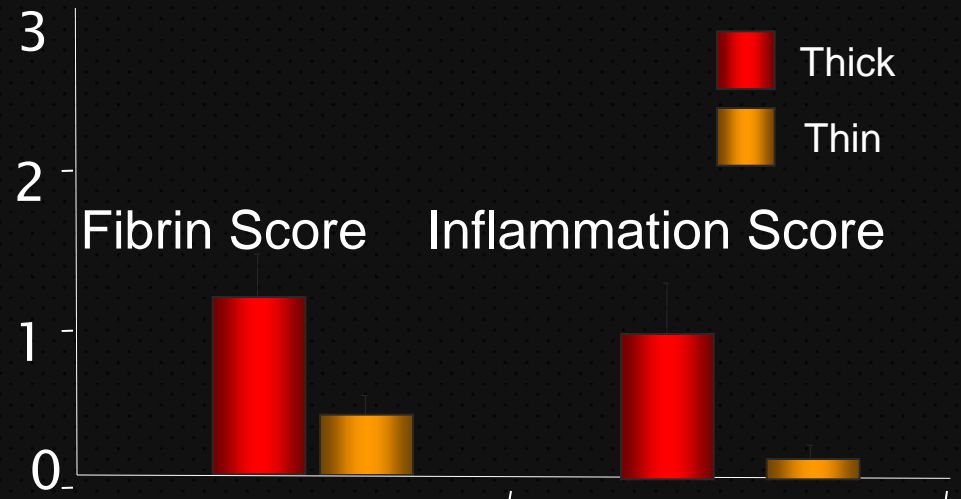
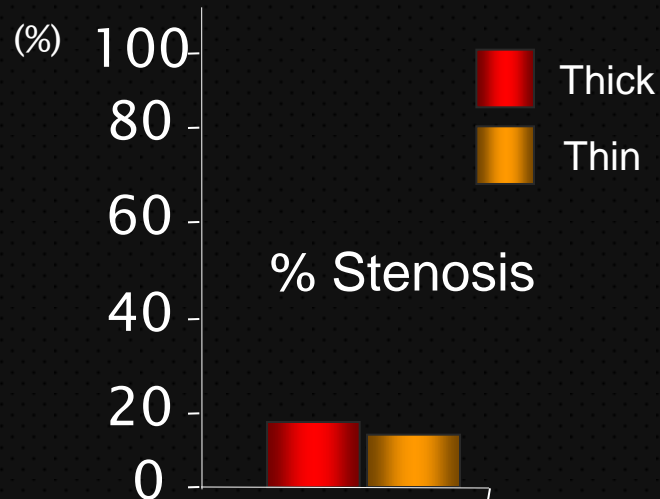
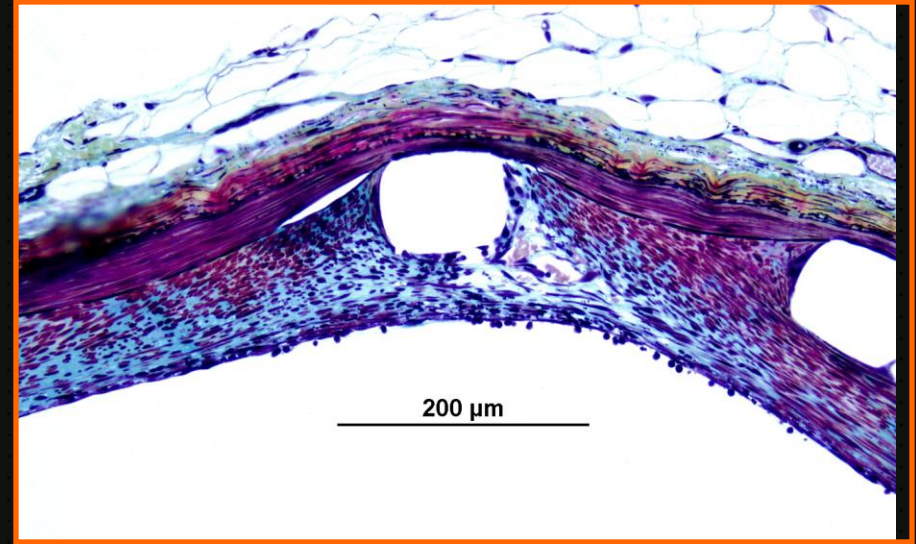
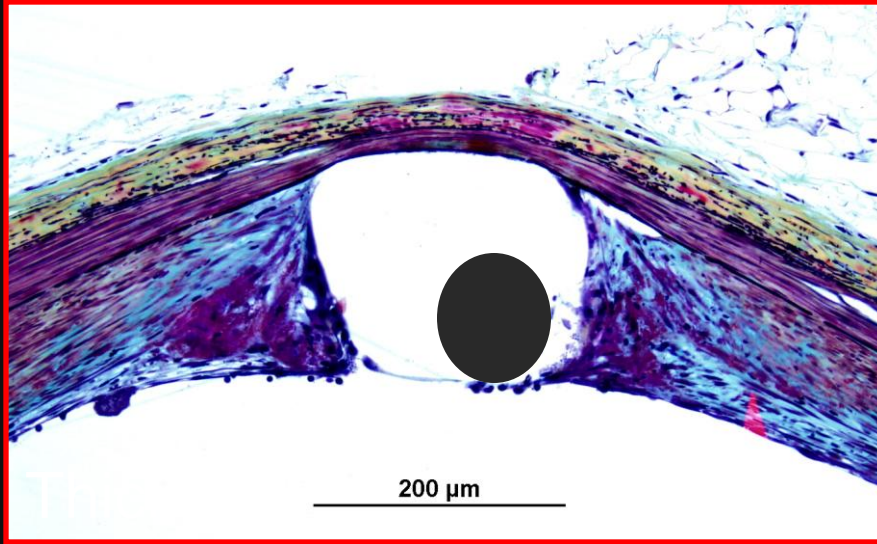
# Impact of Strut Thickness on Vascular Healing and Neointimal Formation in BMS

## Strut Coverage at 14 days in Rabbit



Soucy N, Feygin J et al, EuroIntervention. 2010 Nov;6(5):630–7

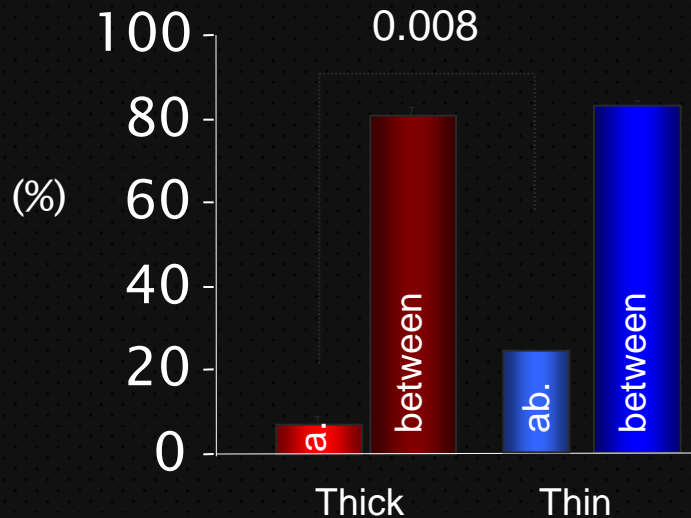
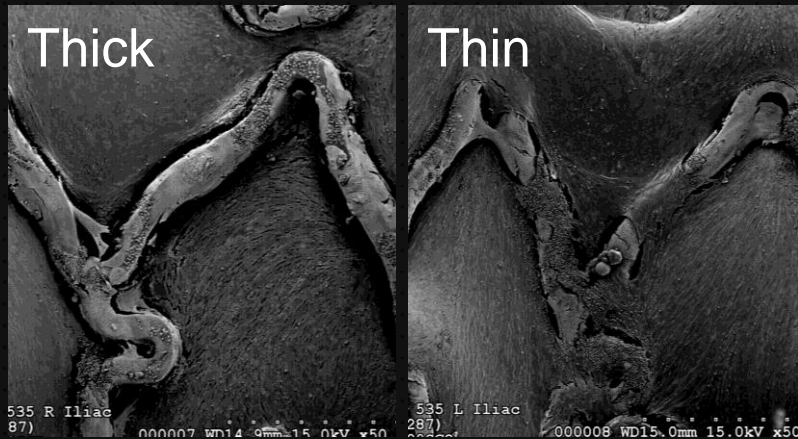
# Optimization of Strut Thickness Leads to Reduction of Inflammation



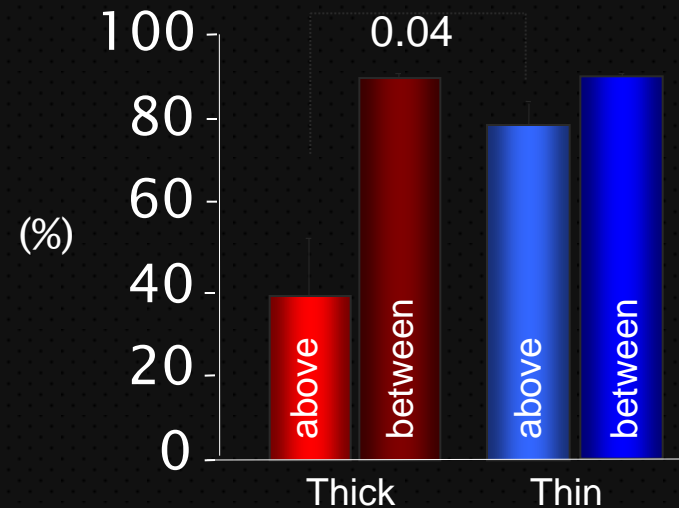
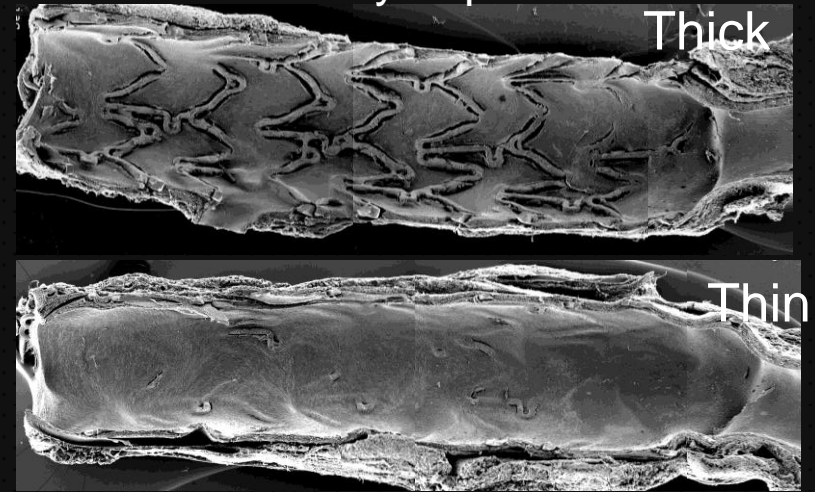


# Optimization of Strut Thickness Leads to Rapid Re-Endothelialization

7-Day Implants

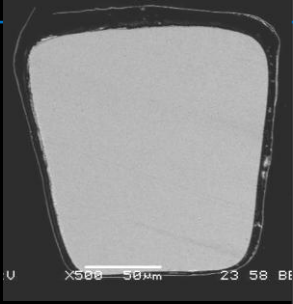
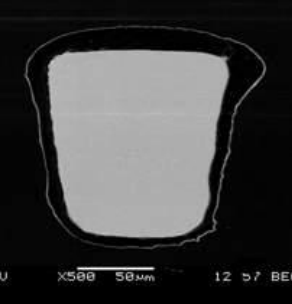
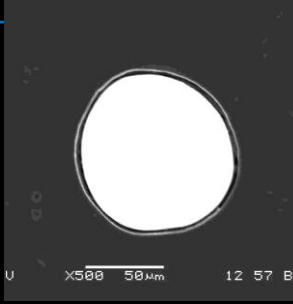
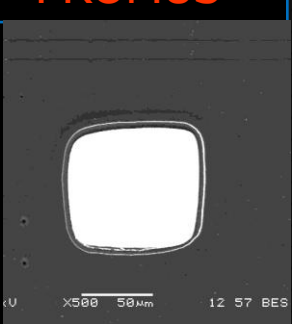
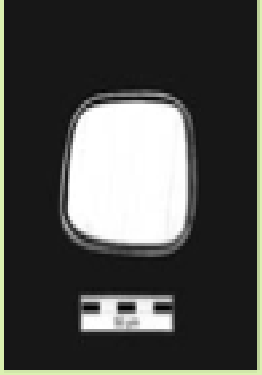


14-Day Implants



Tests performed by and data on file at Abbott Vascular

# Stent Platforms: Strut & Polymer Thickness\*

	CYPHER	TAXUS	ENDEAVOR	XIENCE PROMUS	Orsiro Hybrid DES
Stent					
Strut Thickness	140.0µm	132.0µm	91.0µm	81.0µm	60 µm
Polymer Thickness	12.6µm	16.0µm	5.3µm	7.6µm	7.4 µm
Total	152.6µm	148.0µm	96.3µm	88.6µm	71 µm

\*3.0 mm diameter stents, 500x magnification



# All stents have the following design features

- Hoops provide radial strength
- Connectors hold hoops together and provide longitudinal strength
- Connectors play major role in flexibility

ML8/  
Vision

Element



Biomatrix  
Flex



Driver/  
integrity



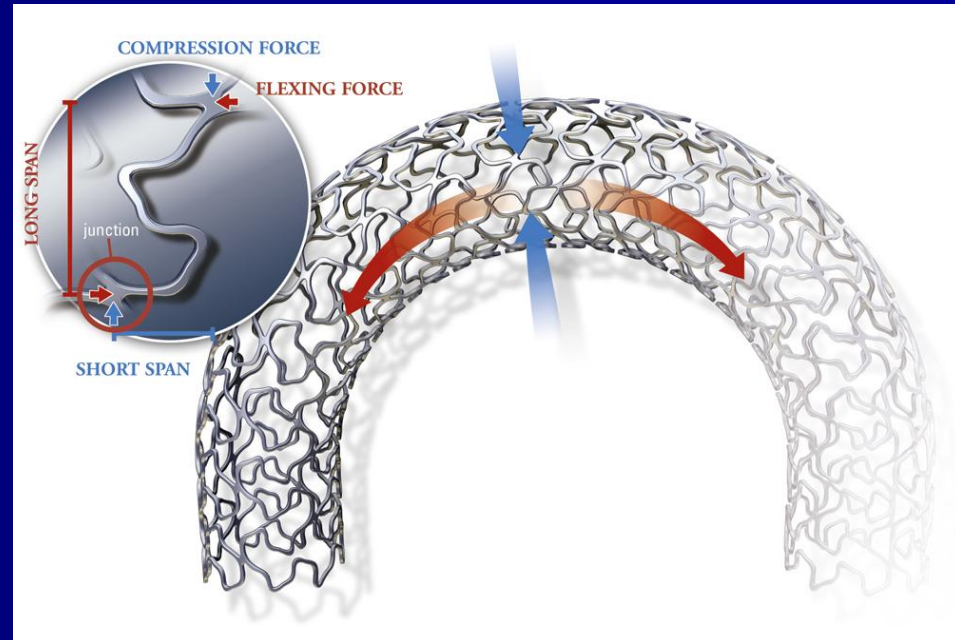
**Bridges/connectors link hoops**

**Welds link hoops**

Ormiston JACC Int 2011

# Design Considerations

- Uniform cell distribution
- Strut dimensions designed to provide radial strength and flexibility
- Continuous cell design and small open cell area provide uniform vessel coverage
- Thin struts for flexibility



# Everolimus-Eluting Stents

## Xience V™ and PROMUS Element™

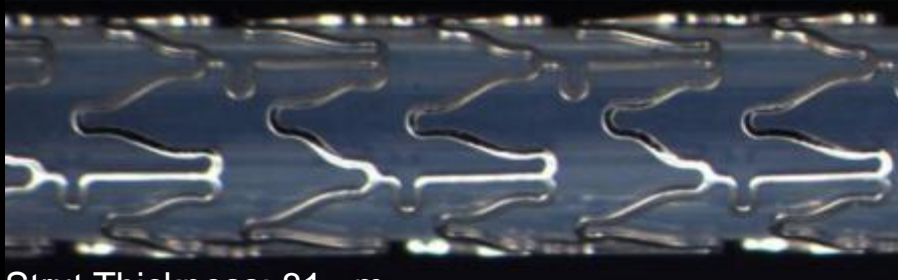
Same Drug and Polymer

Everolimus concentration: 100 ug/cm<sup>2</sup>

Polymer: PVDF

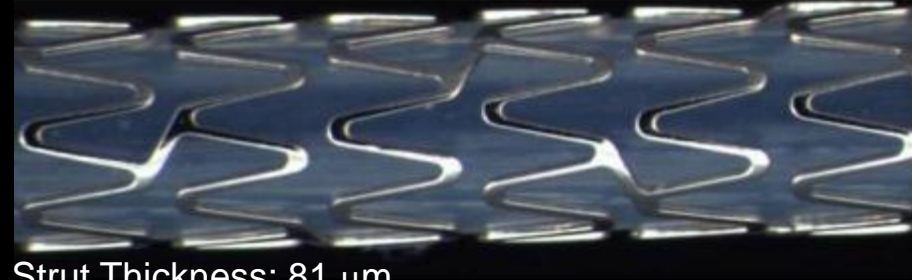
Polymer Thickness: 8 μm

Xience V™ Stent

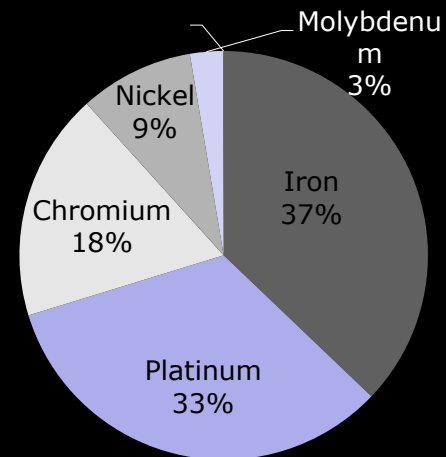
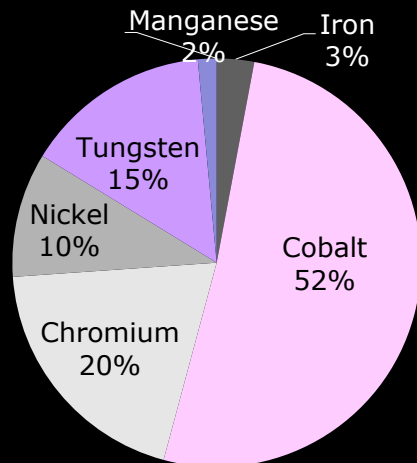


Strut Thickness: 81 μm

PROMUS Element™ Stent

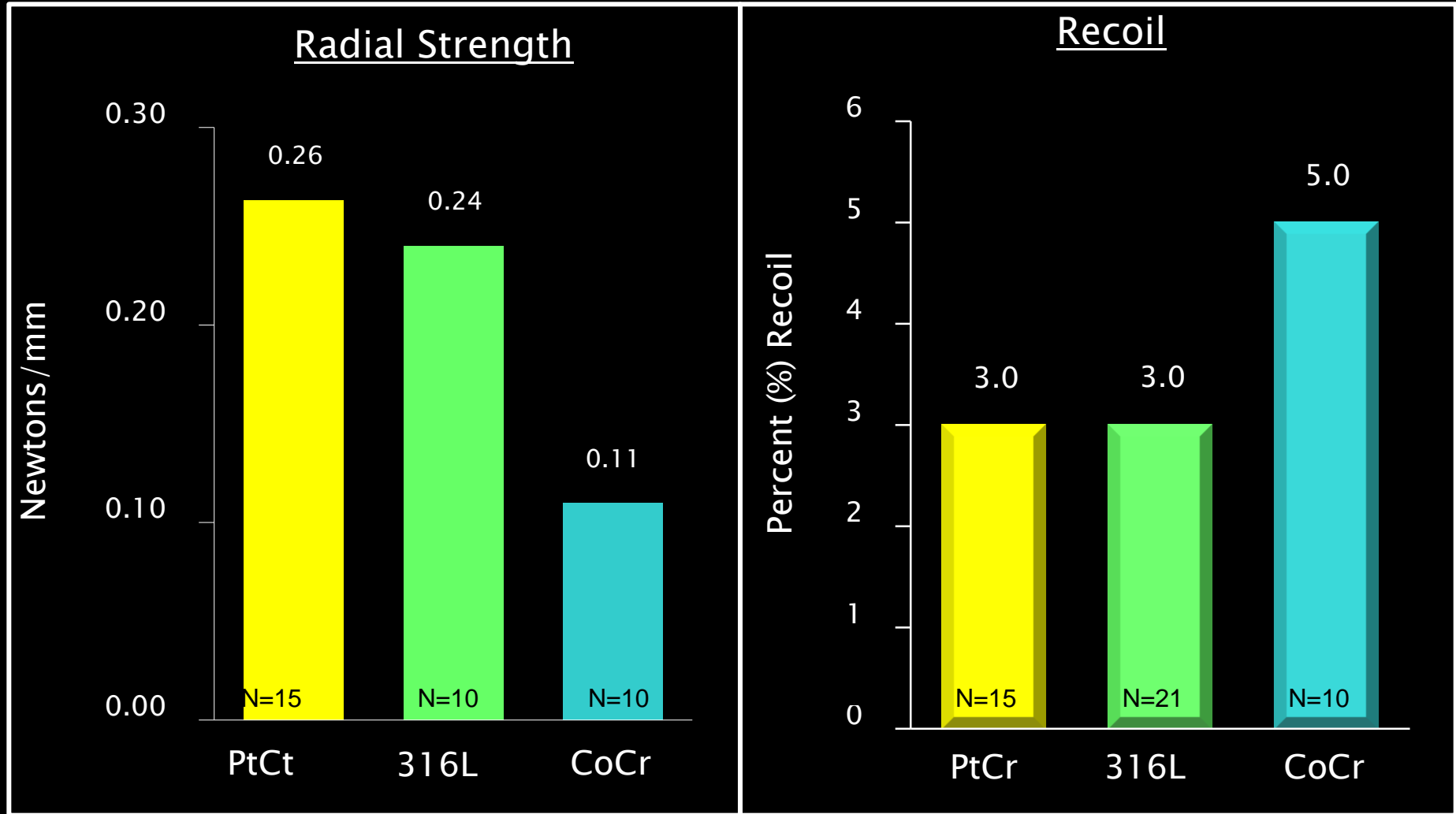


Strut Thickness: 81 μm



# Radial Strength and Recoil

## Bench Test Data



PROMUS Element™ Stent



TAXUS Liberte™ Stent

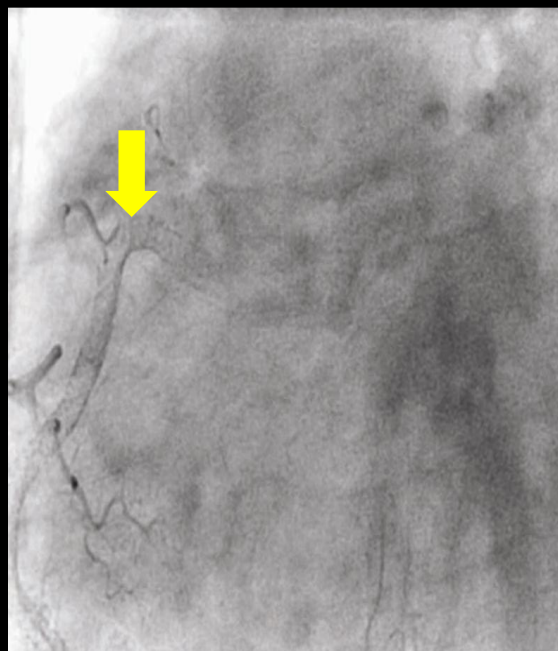


Xience V™ Stent

Data on file at Boston Scientific. 2.5mm diameter stents. Bench test results may not be indicative of clinical performance.

# PROMUS Element™ Stent

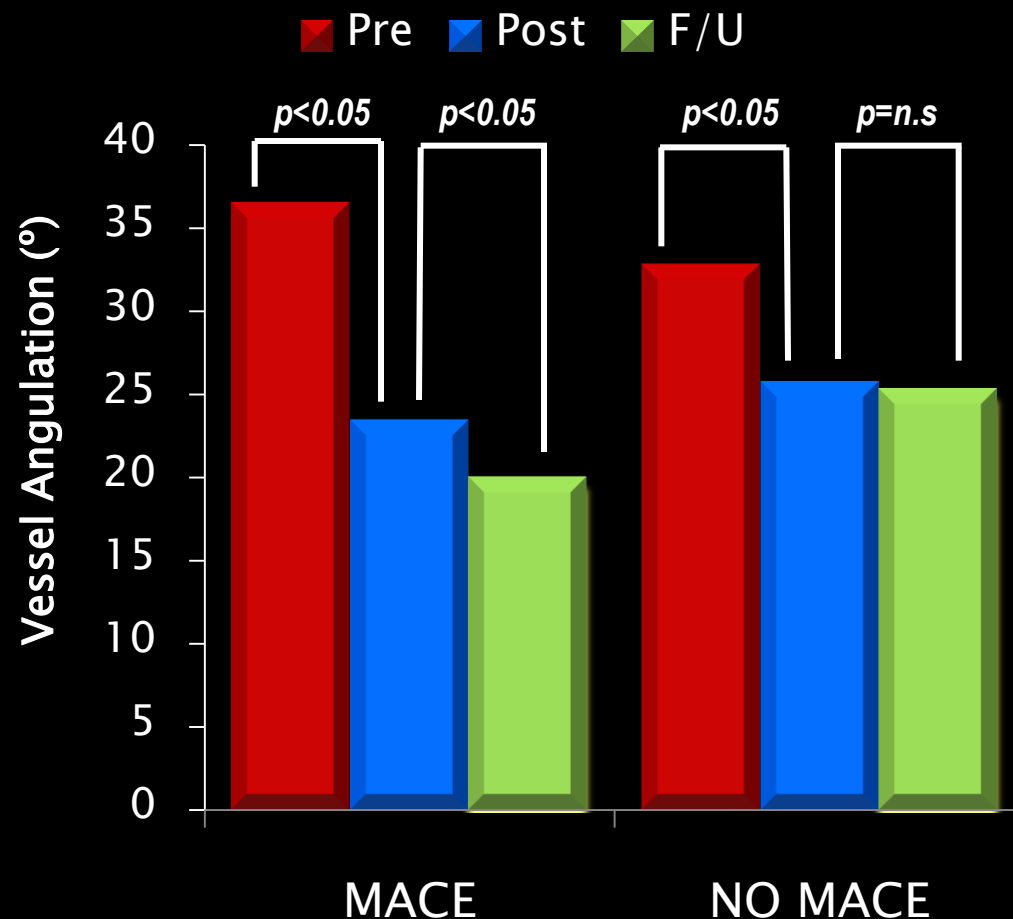
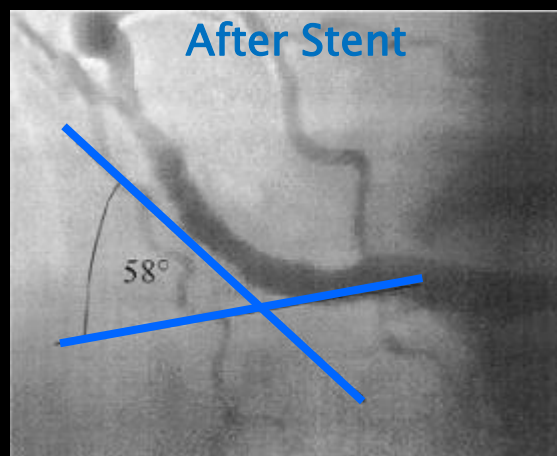
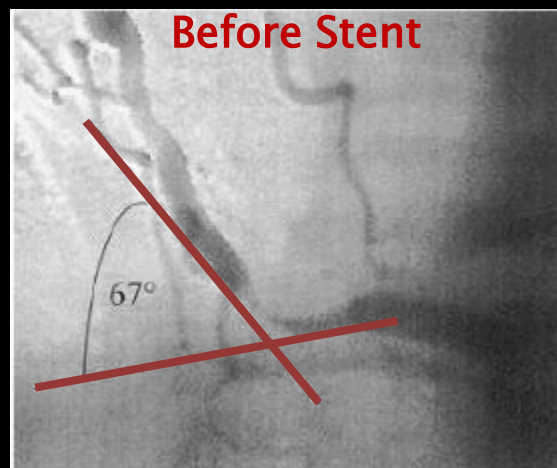
Conformable platform allows artery to retain natural curvature



# Vessel Angulation and Straightening

Pronounced straightening of stented artery associated with MACE

Measurement Methodology

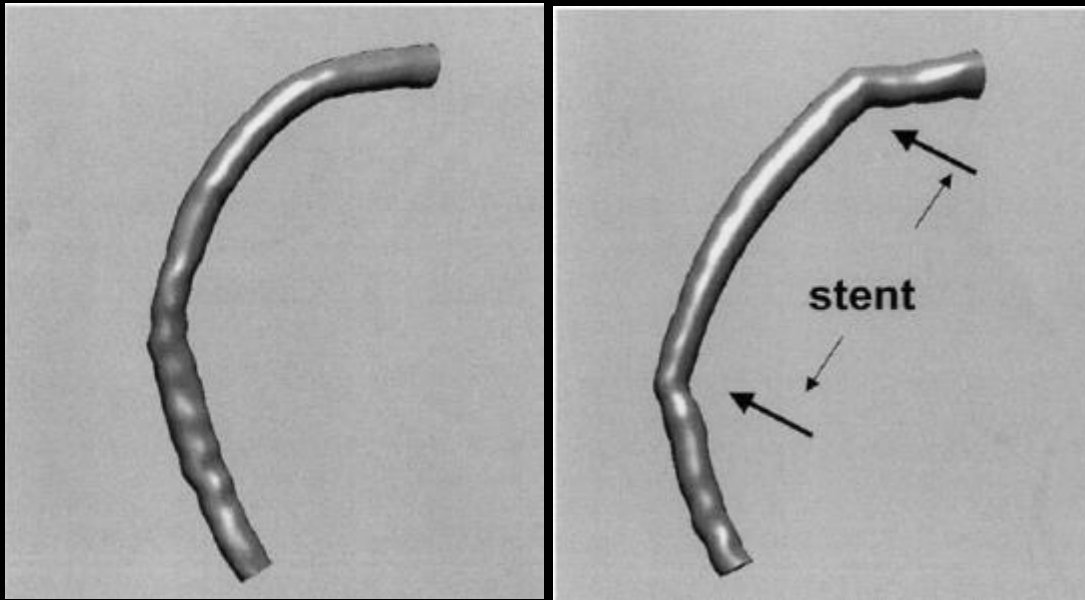


Pre-stent vessel angulation  $\geq 33.5^\circ$  and change in vessel angulation post-stent  $\geq 9.1^\circ$  found to be significant predictors of MACE



# Edge Effects, Shear Stress, and Restenosis

Shear stress changes may affect restenosis



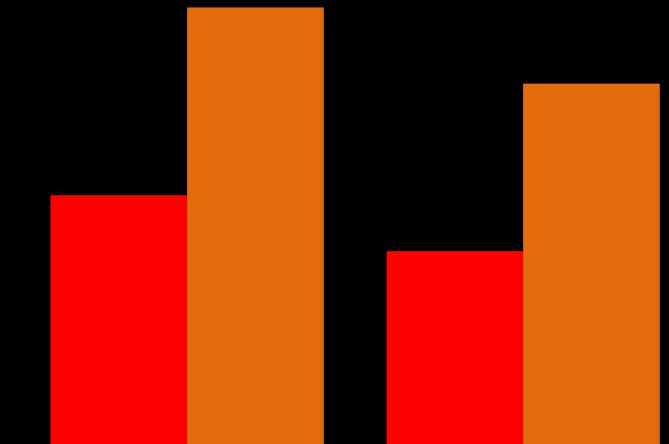
Stent implantation changes 3D vessel geometry  
Changes in shear stress occur near stent edges and  
may result in restenosis

Changes in shear stress and flow velocity associated with restenosis

Restenosis (n=21)  
No Restenosis (n=246)

$P < 0.001$

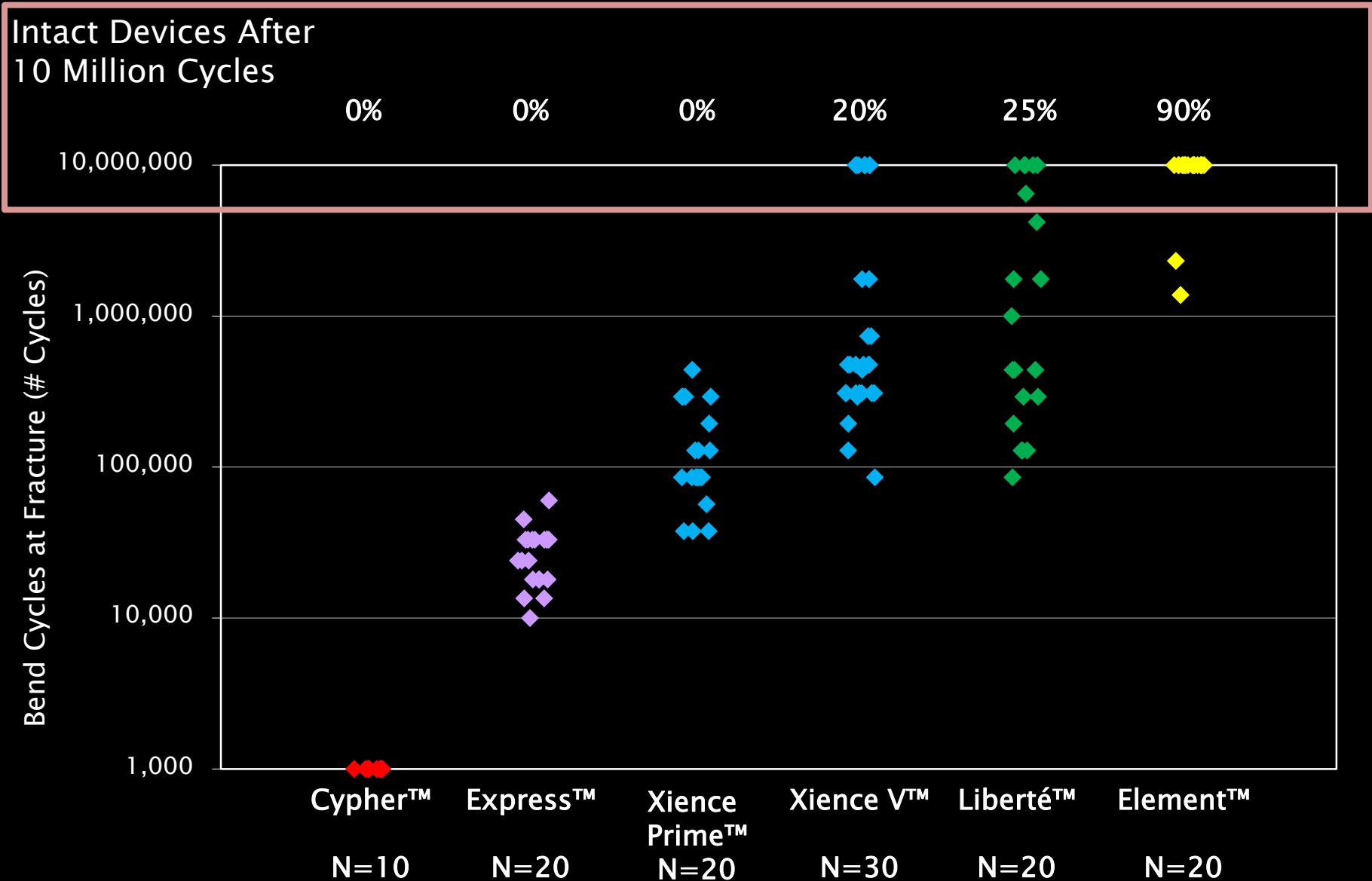
$P < 0.001$



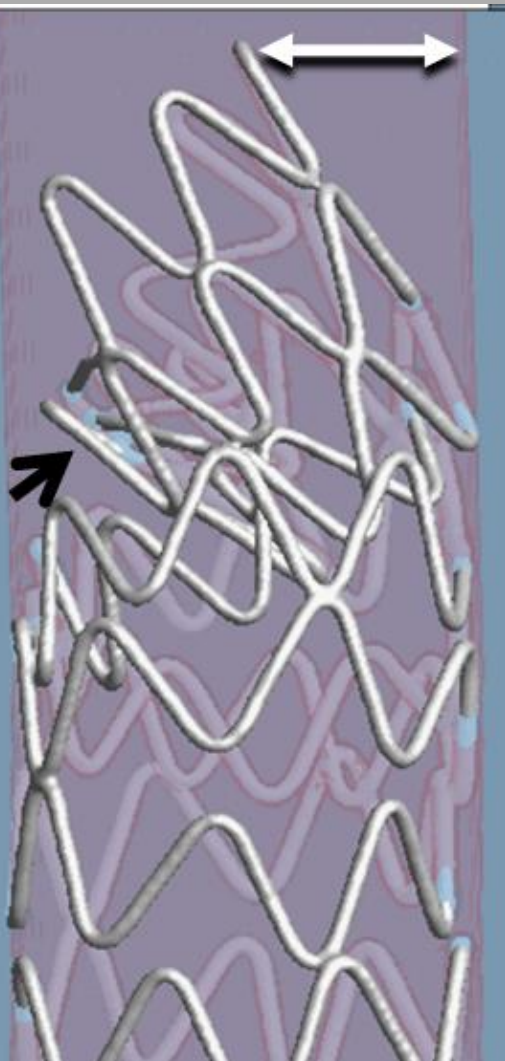
(Shear Stress)

# Increased Fracture Resistance with Flexibility

## Bend Fatigue Bench Test



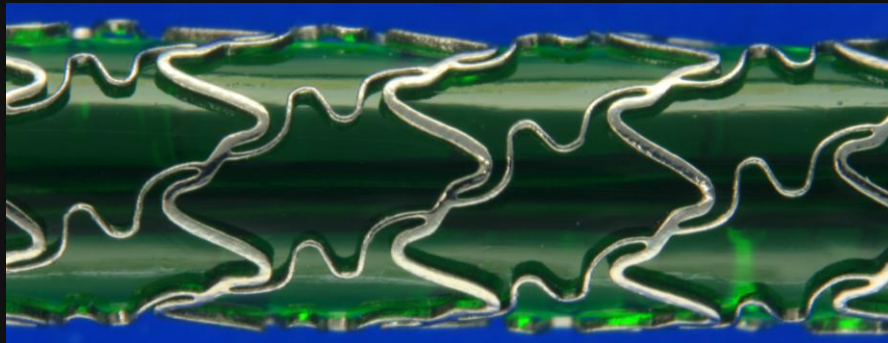
# Longitudinal strength/distortion



- This stent has 2 connectors
- It was distorted by a post-dilating balloon catching a point on the proximal hoop
- Hoops have been pushed together, overlap and obstruct. The proximal hoops are tilted

# Longitudinal strength/distortion

- Stent design is a trade-off and improving one property may be at the expense of a desirable property
- Reducing connectors improves flexibility, SB access and stent fracture potential, it also reduces longitudinal strength



- The Cypher Select stent has 6 connectors linking hoops has high longitudinal strength and low flexibility. Reducing connectors may improve flexibility but at the expense of longitudinal strength

# First Generation Test for Stent Longitudinal Strength-



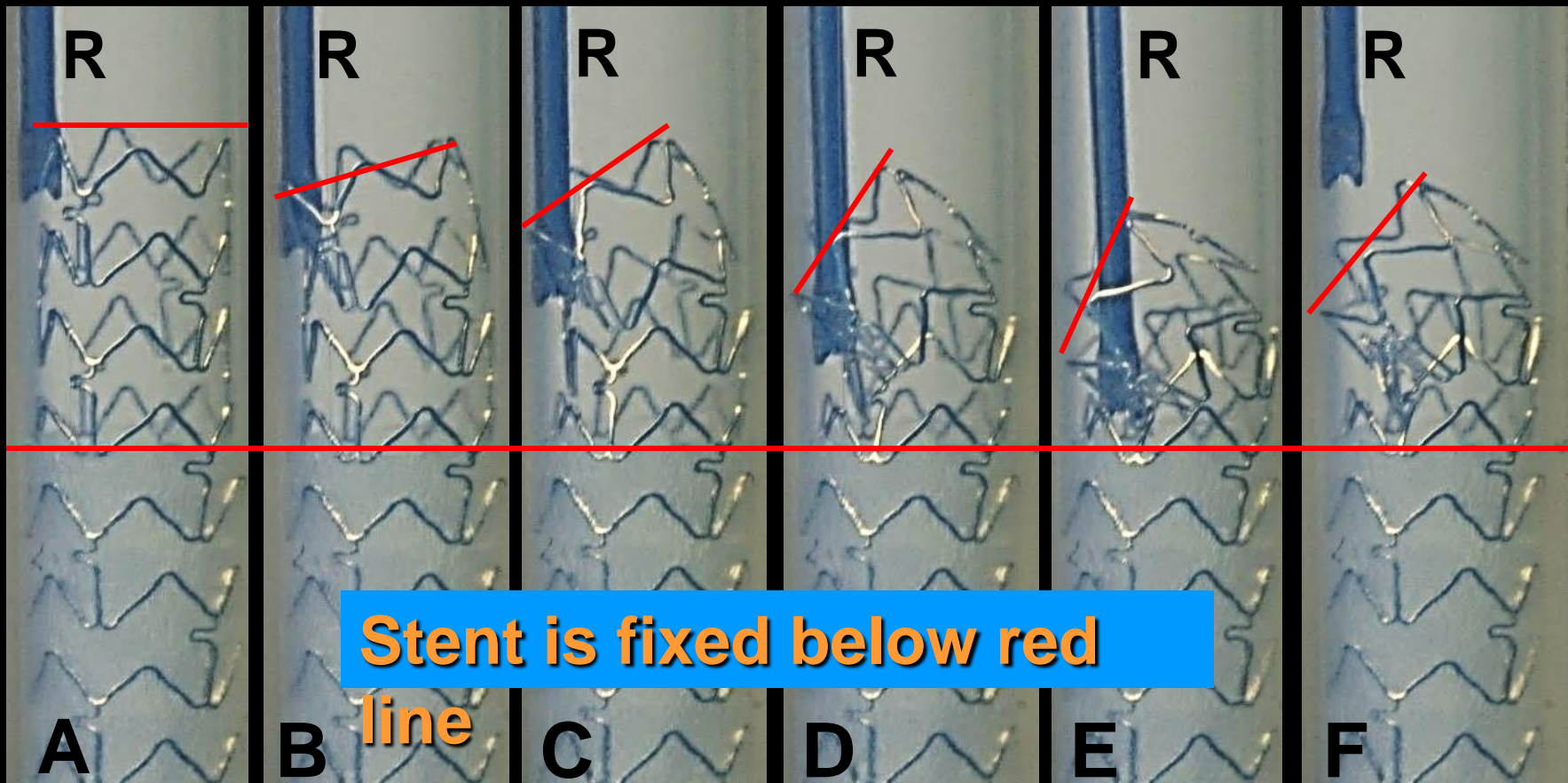
- An instron universal testing machine applied force to the circumference of the proximal hoop
- The force was plotted against distance compressed

*Ormiston JACC Interv  
2011*



## 2<sup>nd</sup> Generation point force compression of a stent

- Stent is fixed distally
- Force from the Instron pushes hoops together and tilts proximal hoop
- Hoops are displaced into and obstruct the lumen
- Struts pulled away from the opposite side are malapposed and obstruct
- Instron measures force and distance





# Reported Longitudinal Stent Deformation

## Described with at least 12 stents

### BioMATRIX™ Stent

Hanratty EuroIntervention, 2011  
Williams, EuroIntervention, 2011

### Micro Driver™ Stent

Pitney, EuroIntervention, 2011  
Mammas, EuroIntervention, 2012

### Resolute Integrity™ Stent

Hanratty EuroIntervention, 2011

### TAXUS™ Liberté™ Stent

Williams, EuroIntervention, 2011  
Mammas, EuroIntervention, 2012

### Endeavor™ Stent

Pitney, EuroIntervention, 2011  
Mammas, EuroIntervention, 2012

### PROMUS Element™ Stent

Hanratty EuroIntervention, 2011  
Williams, EuroIntervention, 2011  
Mammas, EuroIntervention, 2012

### ION™ / TAXUS Element™ Stent

Robinson, J Interv Cardiol, 2011  
Mammas, EuroIntervention, 2012

### Xience V™

Olcay, TCT 2011  
Mammas, EuroIntervention, 2012  
Yamaguchi, JACC, 2012

### OMEGA™ Stent

Mammas, EuroIntervention, 2012

### Driver™ Stent

Mammas, EuroIntervention, 2012

### Cypher™ Stent

Mammas, EuroIntervention, 2012

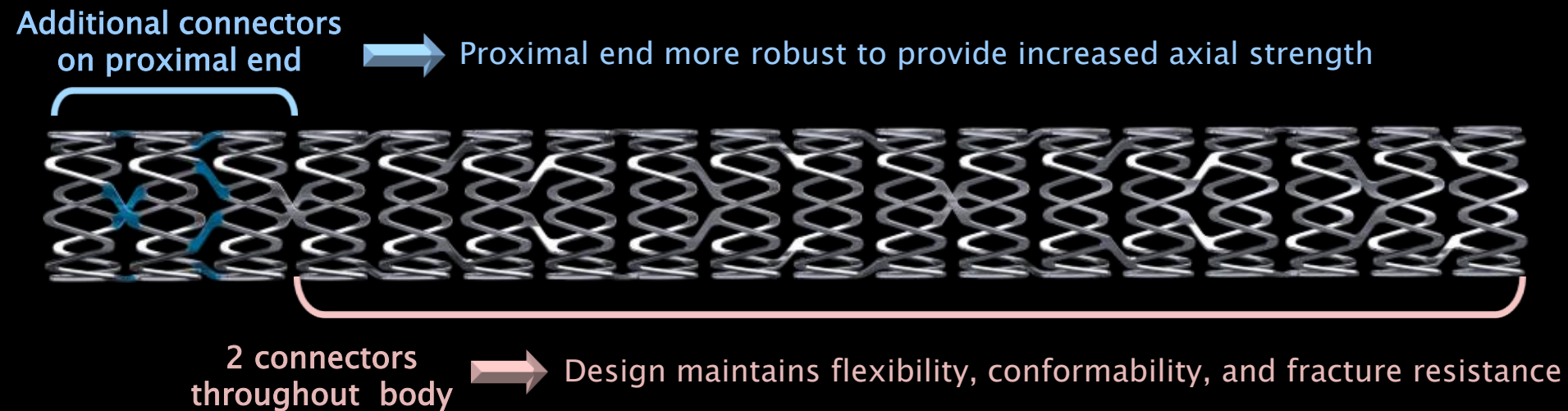
### Nobori™ Stent

Mammas, EuroIntervention, 2012

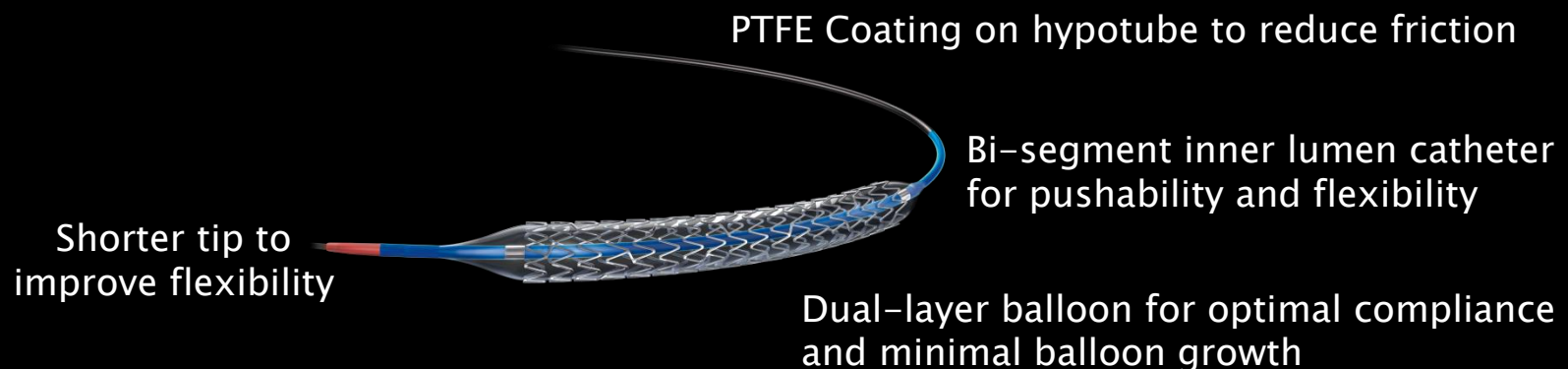
Most reports have been restricted to anecdotal case reports

# Promus PREMIER™ Everolimus–Eluting Stent Design Goals

## Customized Platinum Chromium (PtCr) Stent Architecture

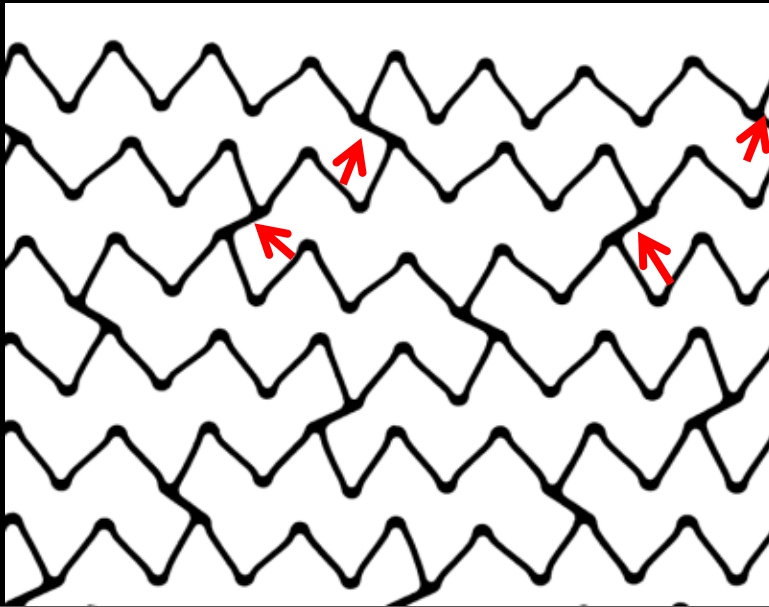


## Enhanced Stent Delivery System



# Promus PREMIER™ Stent

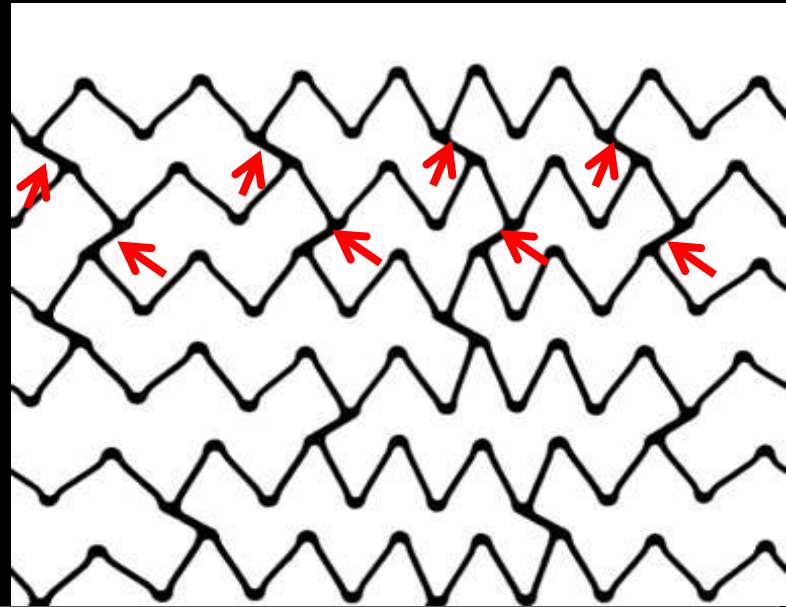
- Promus PREMIER design improves longitudinal strength by supporting proximal end with additional connectors where distortion most commonly occurs
- Delivery system improved
- Retains the desirable features of the Element design (flexibility, conformability, radiopacity)
- No change to drug or polymer



Element Design

- 2 connectors between hoops

John Ormiston, MD at CRT 2013



Promus Premier design

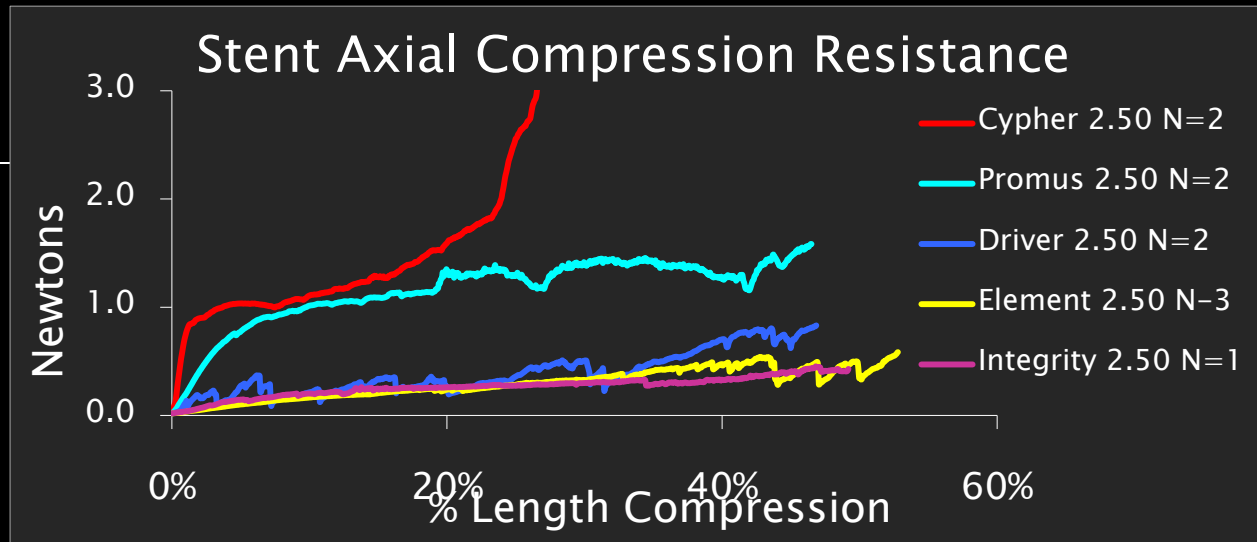
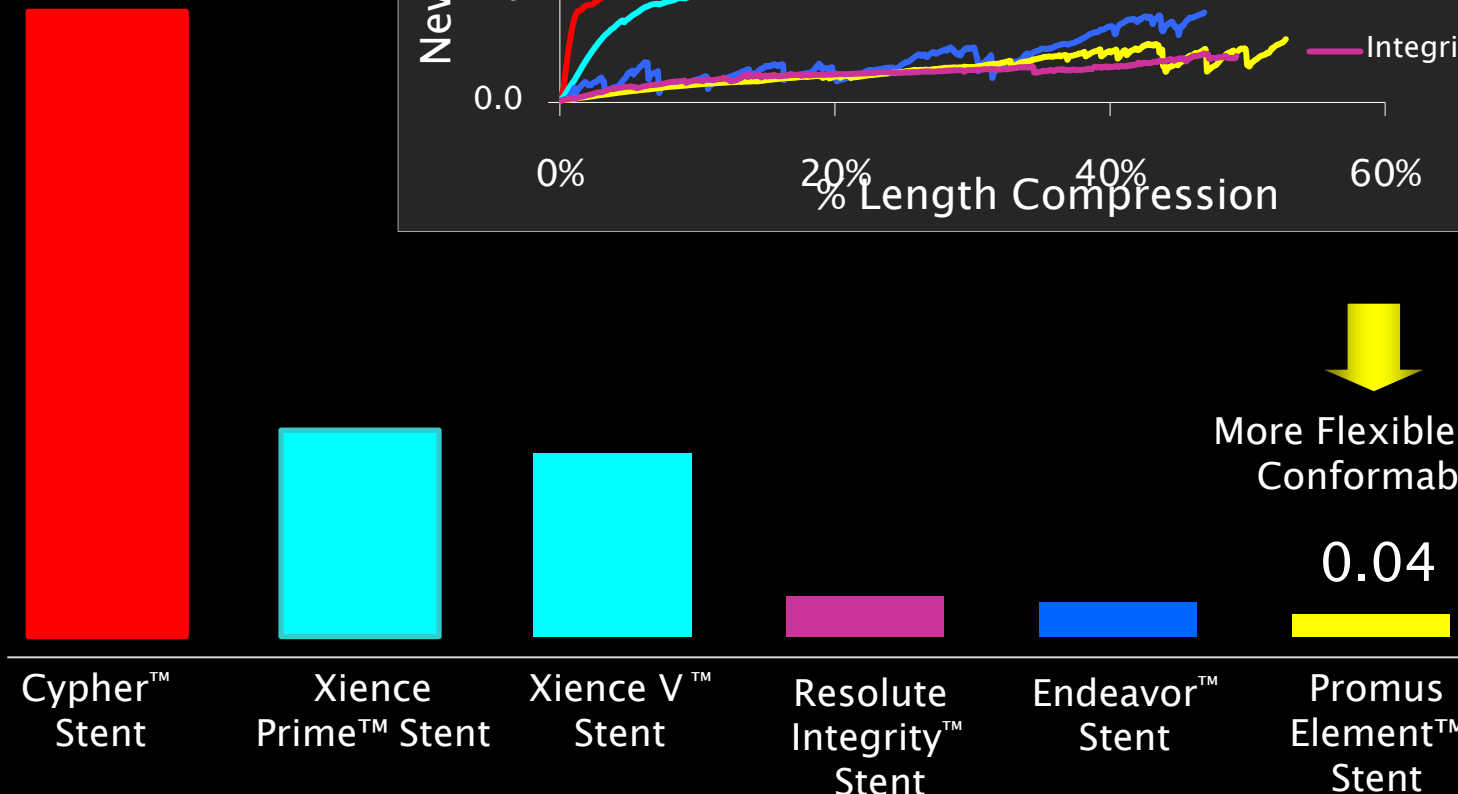
- 4 connectors between proximal 3 hoops.
- 2 connectors between remaining hoops.

# Flexibility and Conformability

## Flexibility & conformability inversely related to axial strength

### Flexibility/Conformability Bench Test

Bending Moment  
(Newtons · mm)

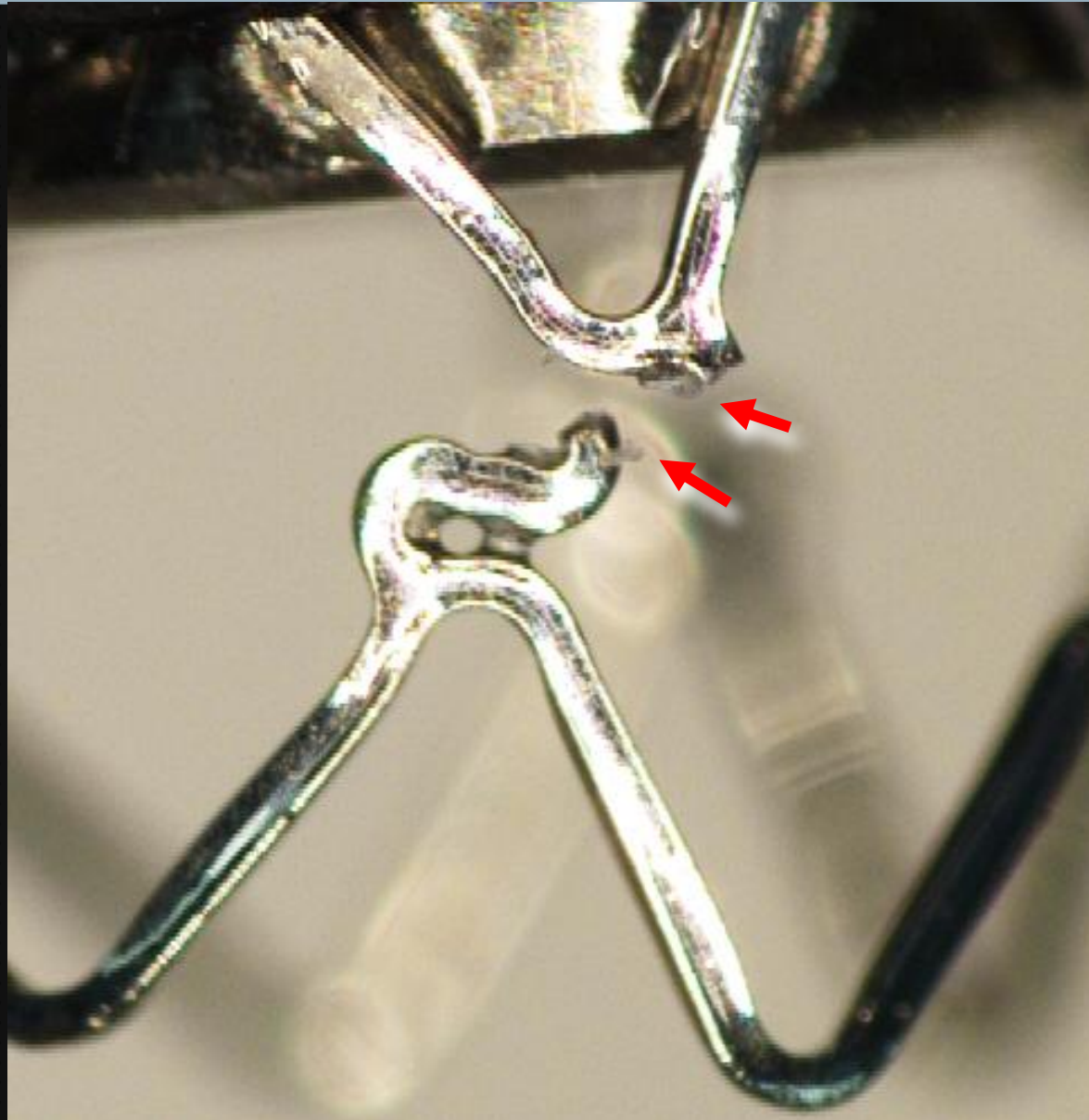


More Flexible and Conformable

0.04

# Stent strut fracture

(and damaged resorbable polymer)



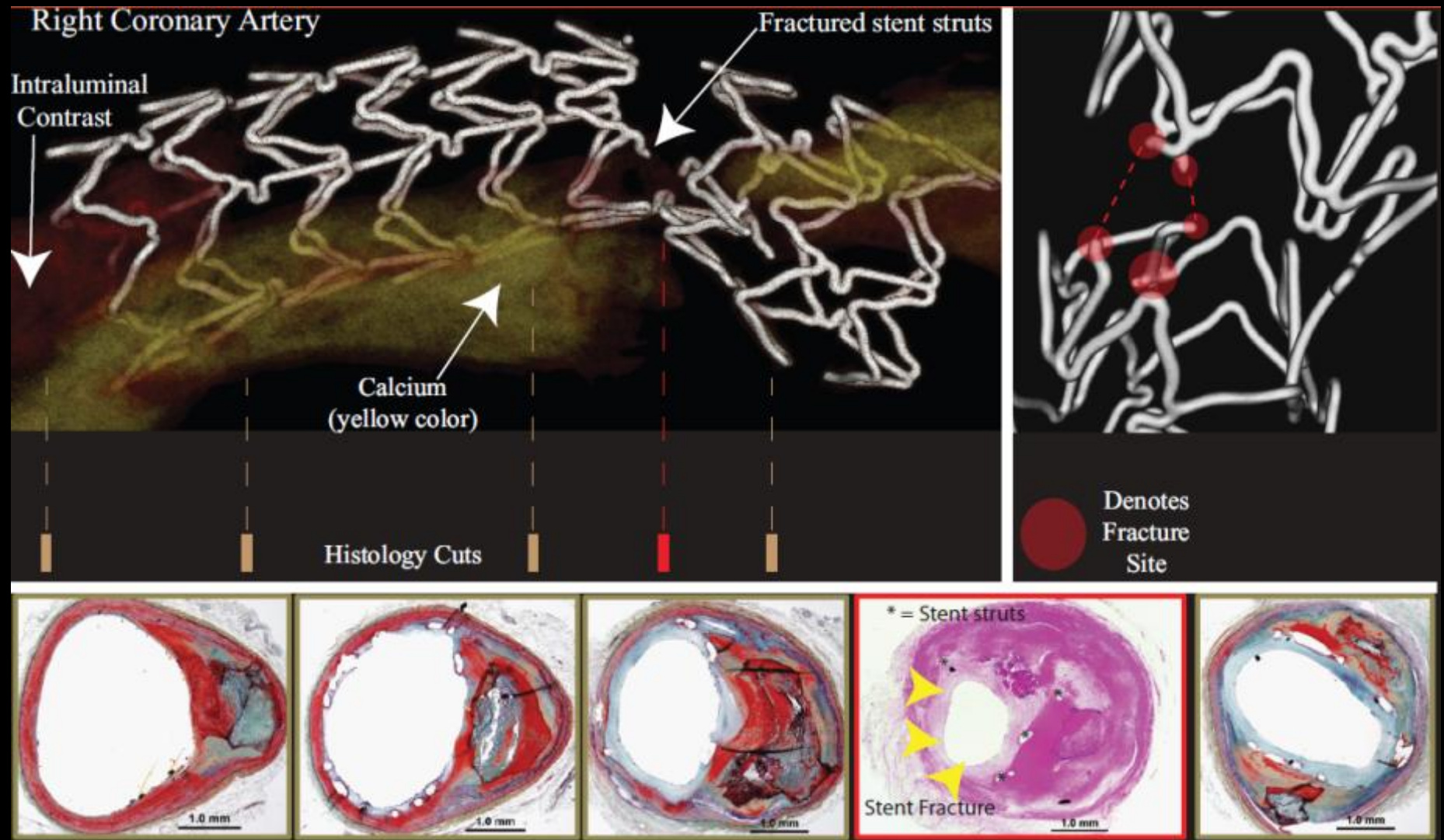
# Stent fracture

- Recognized for at least 10 years (Chowdhry, NEJM 2002)
- Associated with MACE ( may cause of ST, restenosis, late “catch up”)
- Meta-analysis of 8 studies with 5321 patients and 108 stent fractures incidence of fracture was 4% (All but one were in Cypher)  
(Charkravarty, AJC 2010)
- The probability of fracture is increased with long stents, overlapping stents, RCA, bend points, DES, stent design
- Recent single center report  
Xience V implanted in 1339 lesions  
Fracture at 6-9 months in 2.9% lesions, 3.8% patients  
MACE higher in fracture group vs no-fracture (25.6% vs 2.3%;  $P<0.001$ )  
(Kuramitsu, Circ Int 2012)



# Stent Fracture Associated with DES Restenosis

## Human autopsy analysis

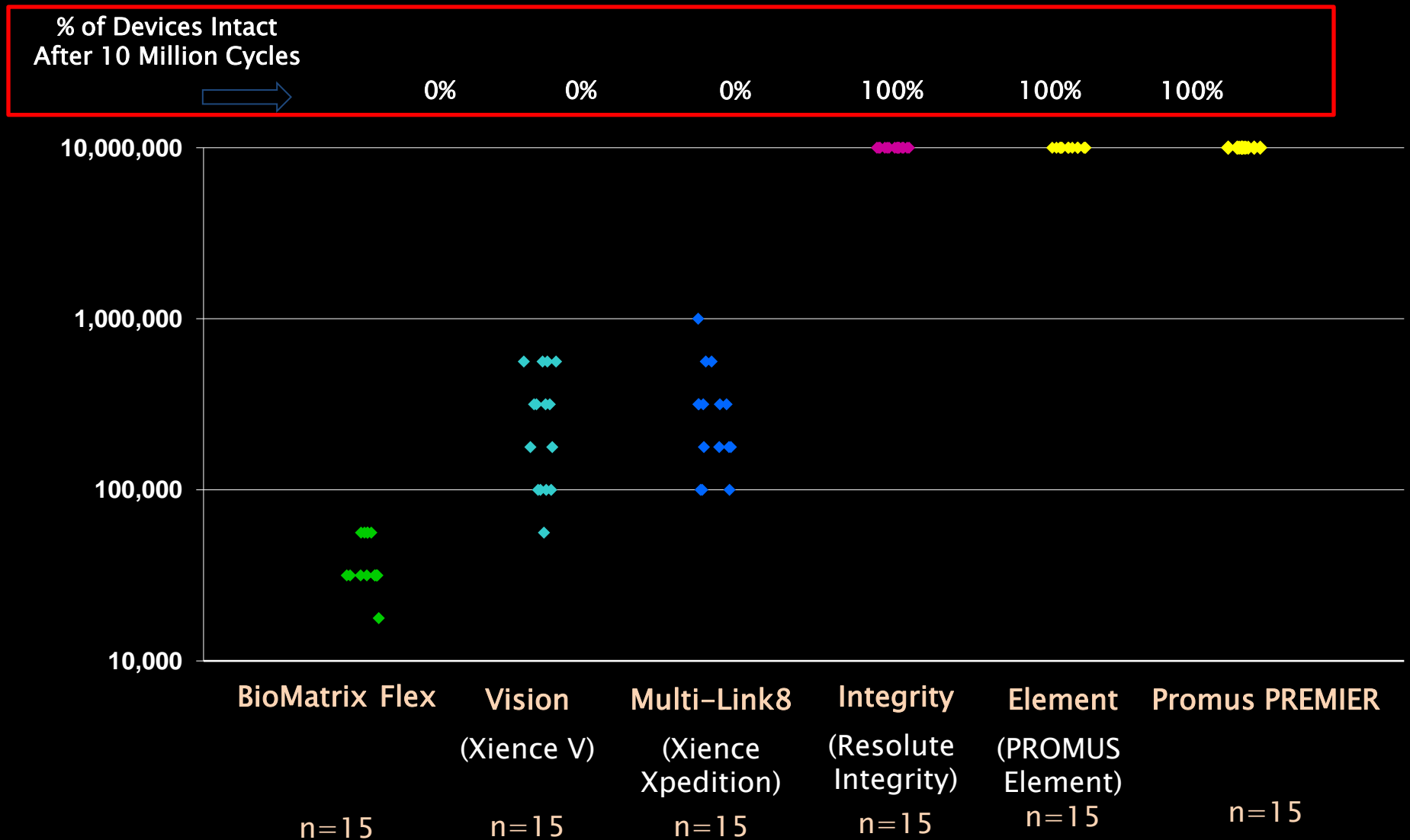


Proximal

Distal

# Stent Fracture

## Bend cycles to fracture for 6 contemporary platforms

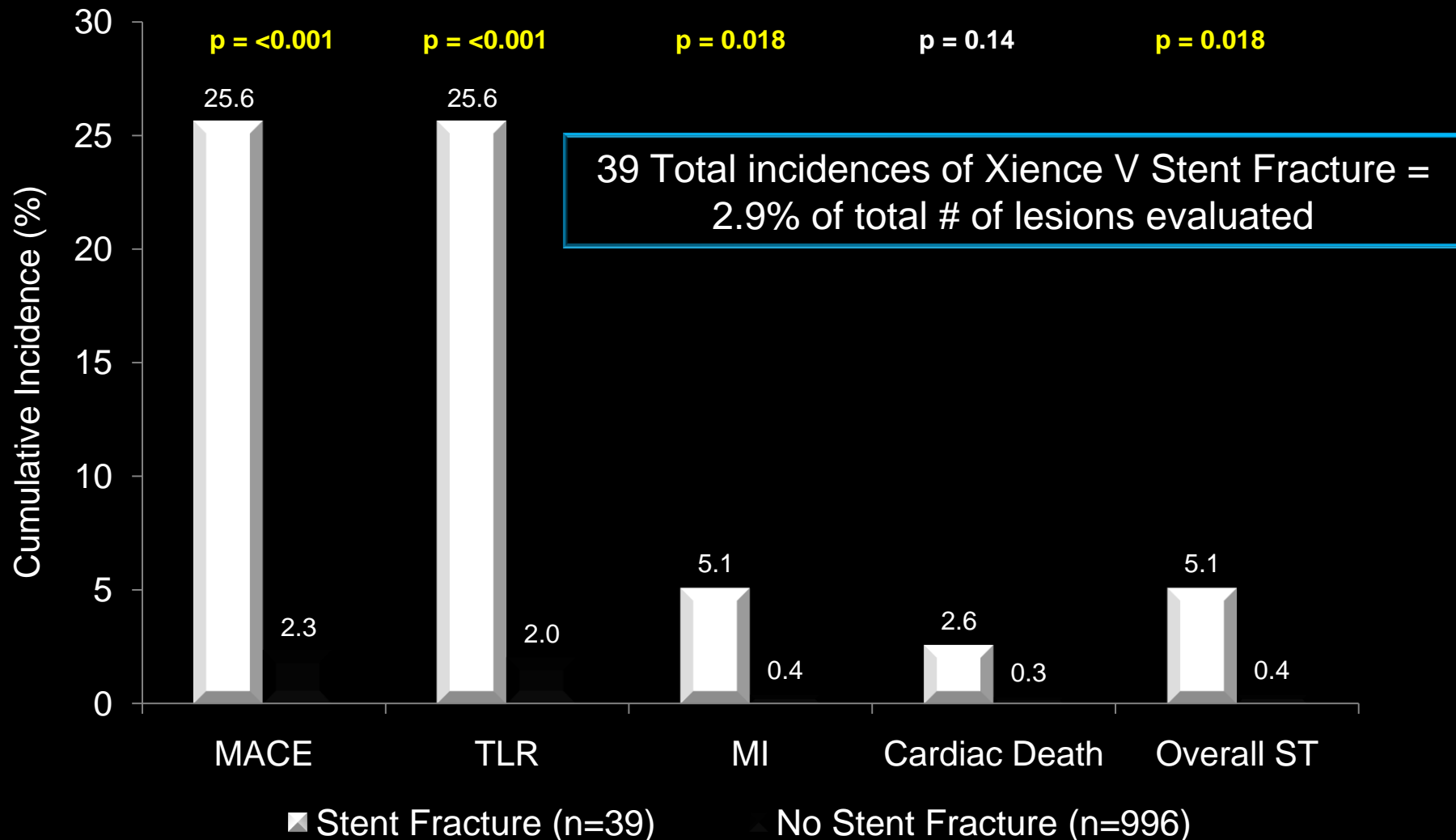


Presented by John Ormiston, MD at CRT 2013

In the United States, Promus PREMIER is an investigational device and not for sale.

# Stent Fracture following Xience V™ Deployment

## Major Adverse Cardiac Events within 9-months

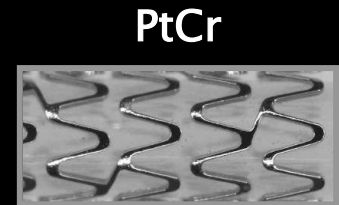
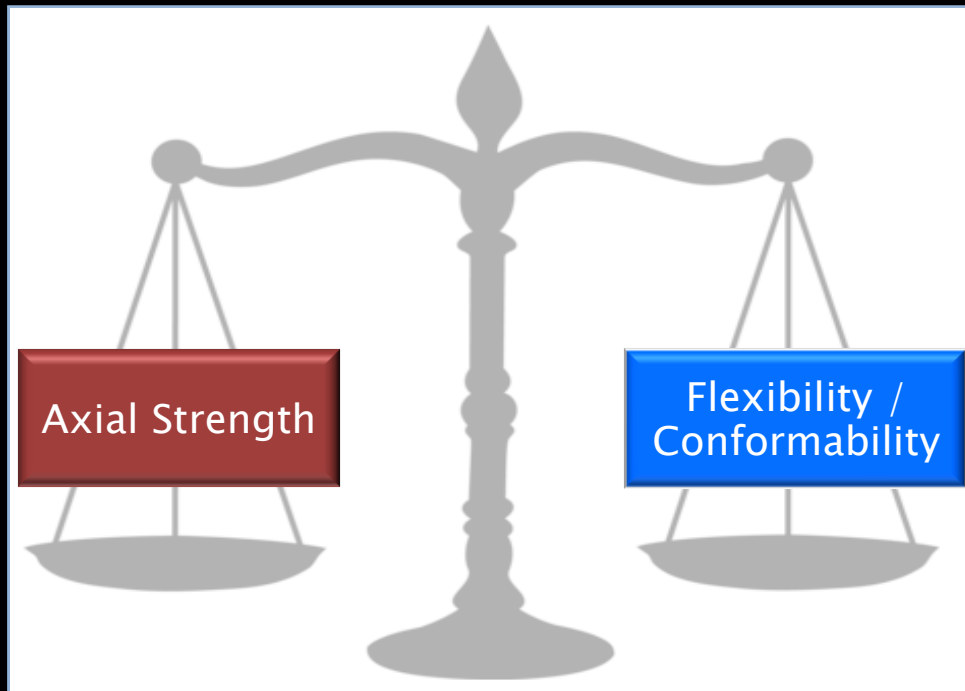


# Flexibility and Axial Strength

## A Balancing Act



Closed Cell



Open Cell



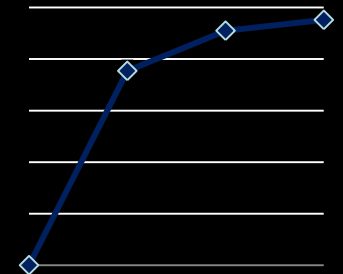
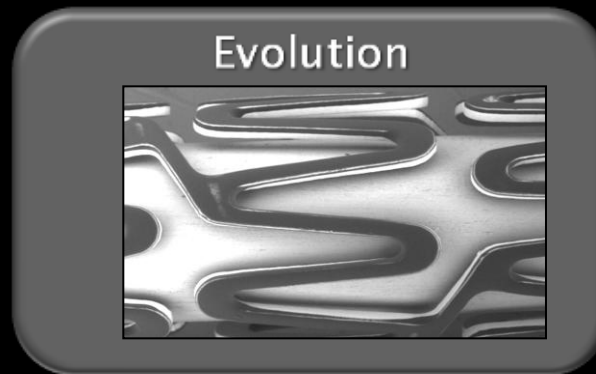
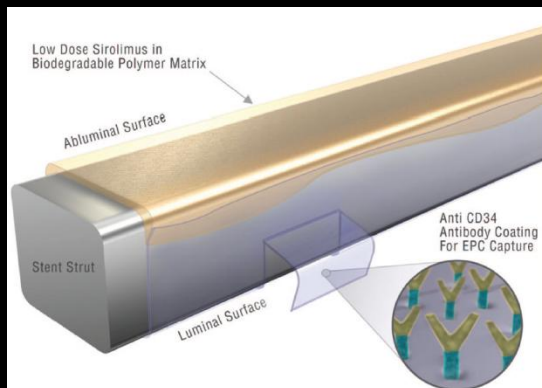
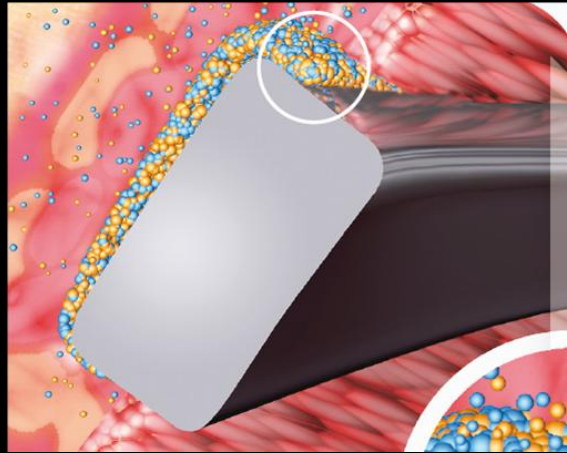
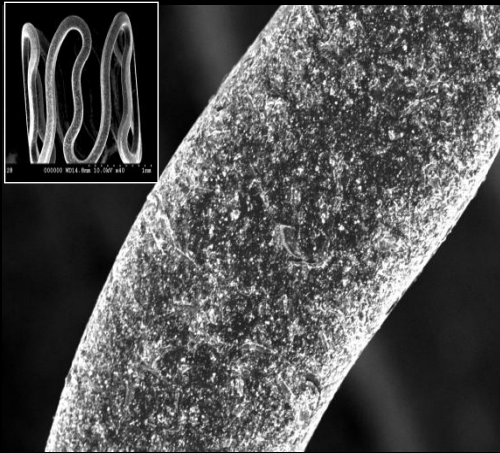
### Greater Axial Strength

- Decreased risk of longitudinal compression

### Greater Flexibility / Conformability

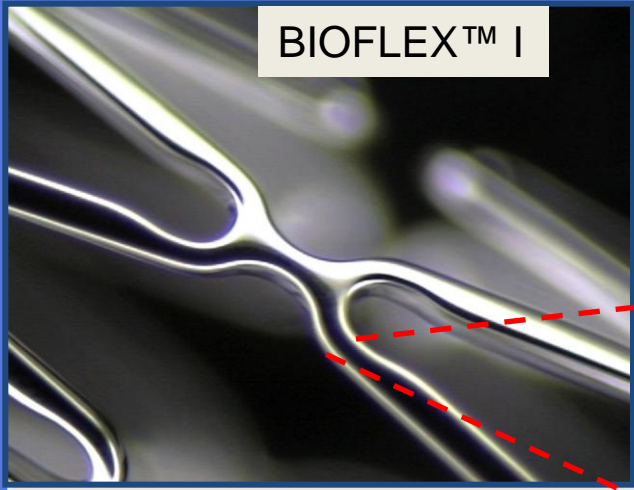
- Improved deliverability
- Lower rates of incomplete apposition
- Less distortion of vessel architecture
- Increased fracture resistance

# Biodegradable Polymer Based DES Platforms





# BioMatrix® II Stent Platform Design

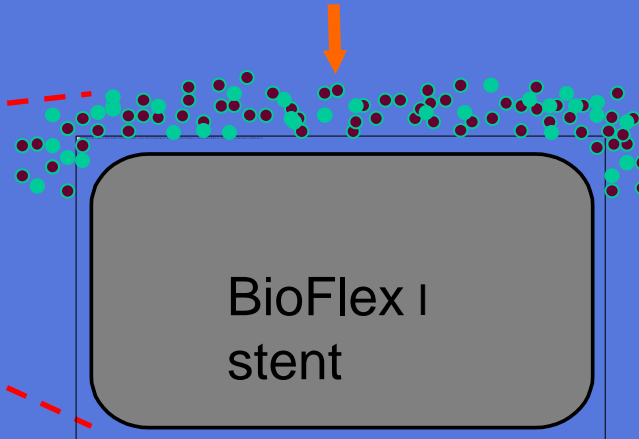


## Stent Platform:

- stainless steel (112  $\mu\text{m}$ )
- corrugated ring, quadrature-link™ design
- radius link enhances axial fatigue life

## Biodegradable Drug/Carrier:

- Biolimus A9® / Poly (Lactic Acid) 50:50 mix
- abluminal surface only (contacts vessel wall)
- 15  $\mu\text{meter}$  coating thickness
- degrades in 9 months releasing  $\text{CO}_2$  + water



## Parylene Durable Primer Coating:

- 5  $\mu\text{meter}$  thick, encapsulates stent
- prevents surface metal ion migration
- biostable + athrombogenic\*

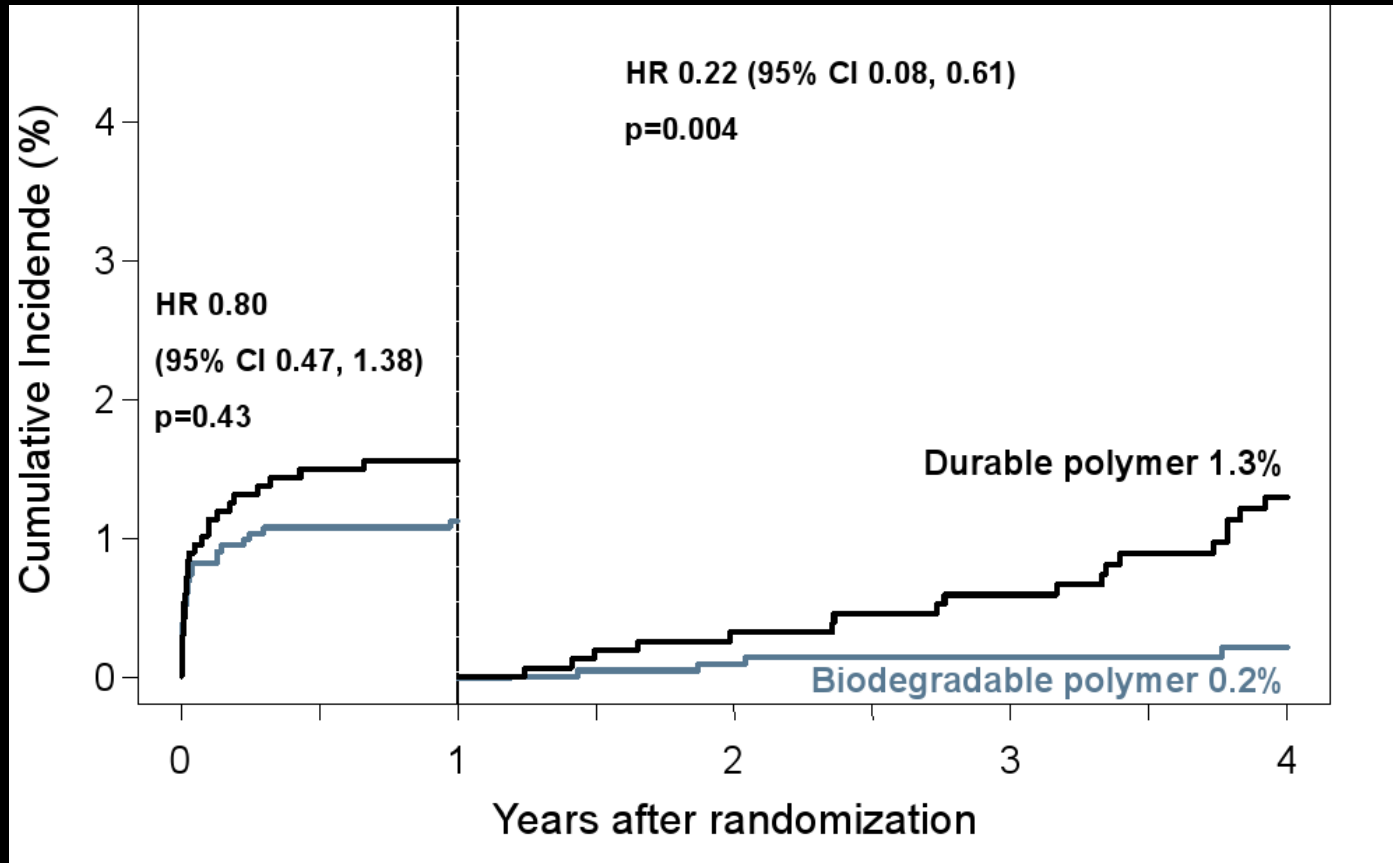
\* Data per NHLBI sponsored study, available from BSI



# Bioabsorbable vs. Durable Polymer DES

## Meta Analysis: ISAR Test-3, ISAR Test-4, & LEADERS

Def ST



# SYNERGY™ Everolimus–Eluting Stent with Synchrony™ Bioabsorbable Coating

Polymer and drug applied as ultra-thin abluminal coating

Synchronized drug release and polymer absorption

Polymer gone shortly after completion of drug elution at 3 months

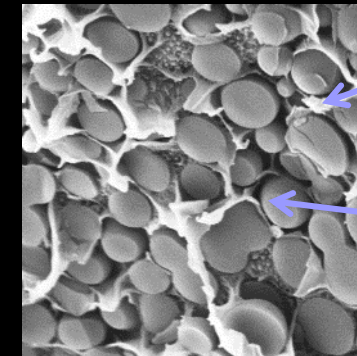
**SYNERGY  
Stent**



**Abluminal  
Coating**



**Coating  
Microstructure**



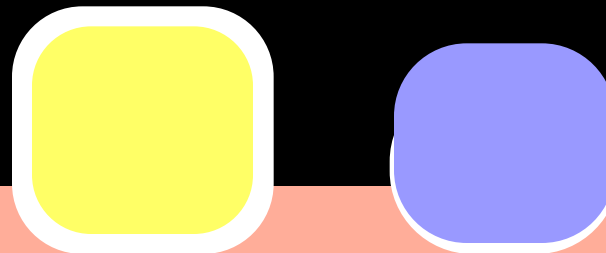
PLGA  
Polymer

Everolimus  
Drug

**Stent Strut Cross Sections**

**PROMUS Element**

PVDF durable  
polymer 360°  
around stent strut



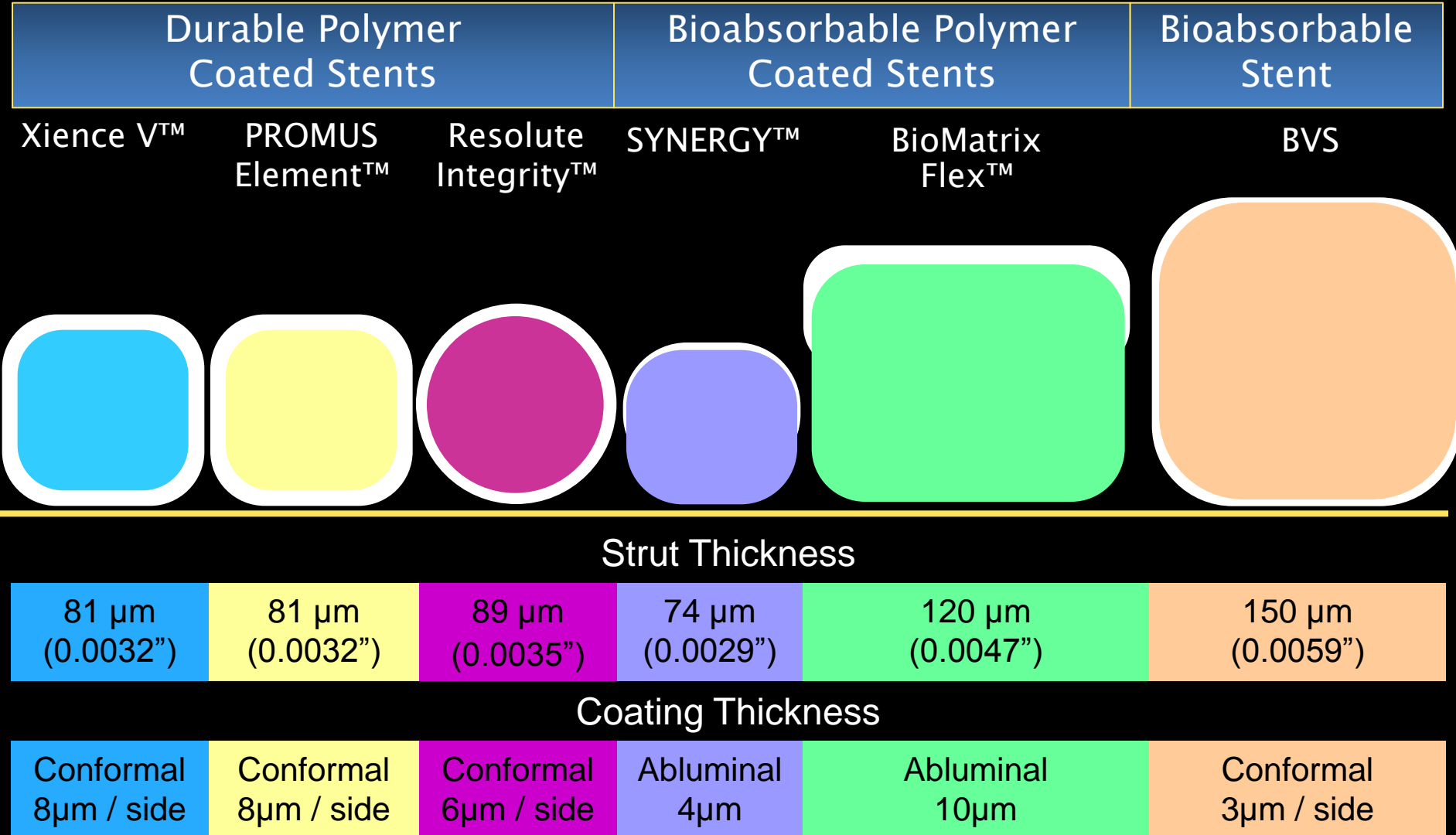
Arterial Wall

**SYNERGY**

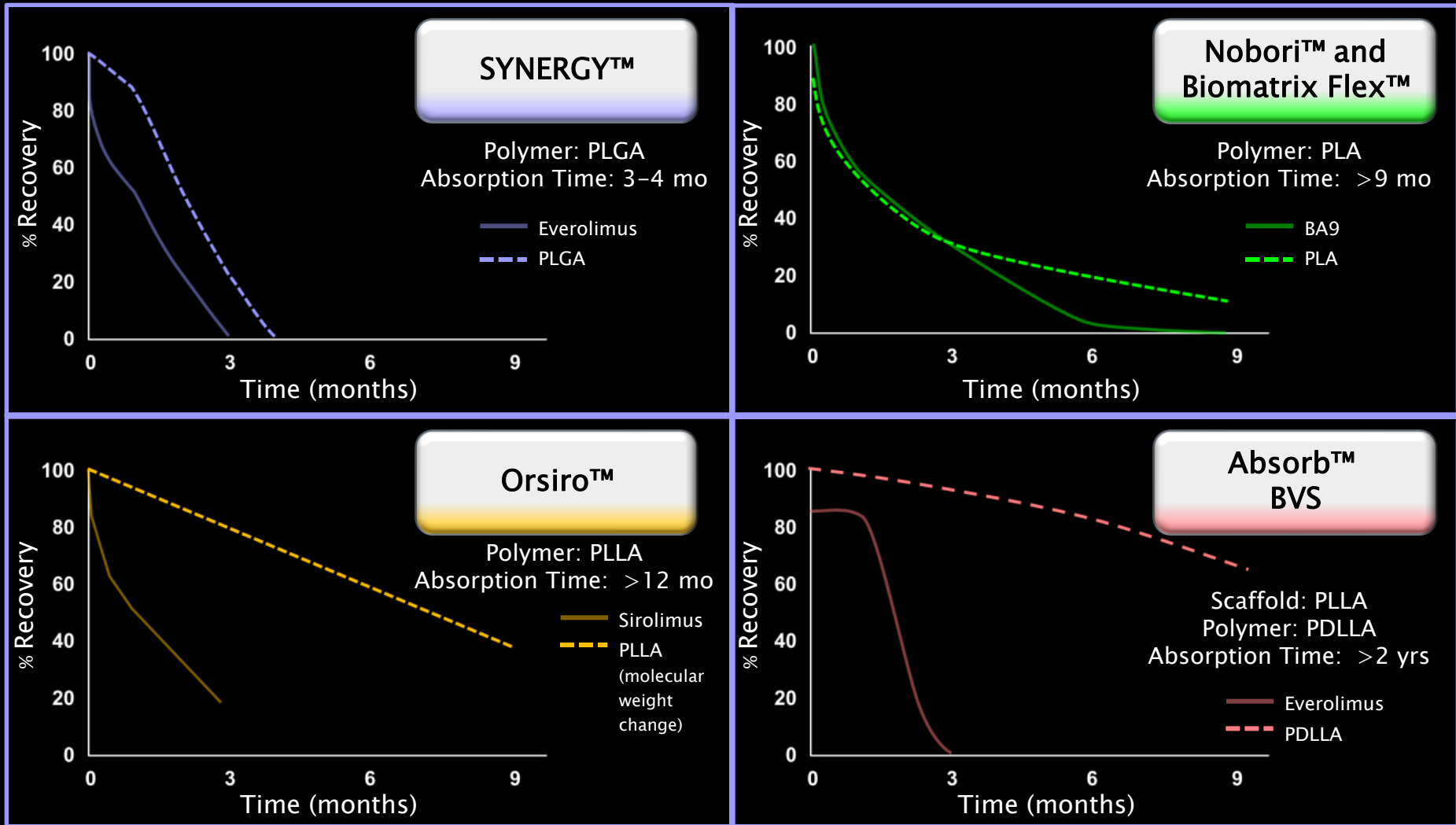
PLGA bioabsorbable  
polymer only on  
abluminal surface

# SYNERGY™ Stent Platform

## Strut and Coating Thickness In Perspective



# Drug Release and Polymer Degradation Profiles



# Summary

- Architecture design have impact on deliverability, flexibility, conformability and deformation
- Two connectors design can easily deformed and require extra care
- Stent fractures occur more in less flexible stents with more connectors & associated with clinical events
- Strut thickness has impact on outcome. The thinner the Better. radial strength may be a limitation
- Polymers has a temporary function for drug elution beyond that they pose hazard to late events
- Thinner biodegradable polymers or no polymers are desire for the next generation DES